

# **A Comprehensive Study on Surface Electromyography Signal Acquisition Procedure for Improving Recognition Accuracy**

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## **ABSTRACT**

In the previous scarcely any years the usage of organic signals as a strategy for interface with a mechanical gadget has gotten progressively increasingly unmistakable. With the a considerable lot of these frameworks being founded on EEG and EMG. EMG based control has five primary parts information obtaining, signal molding, highlight extraction, characterization, and control. This paper sets out to quickly cover the parts of information obtaining for improving acknowledgment precision.

## **I. INTRODUCTION**

Electromyography (EMG) is an electrical sign which is gained from human muscle. EMG signal from human signs are utilized to create hand prosthesis for the individuals who have influenced by upper appendage removal. EMG information can be accumulated in two unique manners: intrusive, and noninvasive. The intrusive technique is performed by embeddings a needle type anode through the skin into the muscle wanted. This method is for the most part utilized for analytic purposes. The intrusive strategy gives high-goals information, and precise restricted portrayals of muscle movement. This technique, be that as it may, causes some distress to the patient, and isn't appropriate for rehashed day by day use. The noninvasive strategy utilizes surface mounted anodes ordinarily situated over explicit muscles. This declines the patient's inconvenience and takes into consideration the capacity to be a completely versatile gadget. This strategy has regularly utilized cements and conductive gels for the mounting of the anodes. In any case, as of late the improvement of surface mounted EMG sensors has made it conceivable to mount sensors without cement or gel. Eventually, this examination explores different procurement technique and discovers better sign obtaining arrangement for improving acknowledgment exactness.

## **II.BACKGROUND STUDY**

(S Constantinos et al., 1995) recorded EMG signals from the biceps brachii muscle at slight intentional withdrawal for five seconds utilizing the concentric needle terminal. The cathode was embedded at any rate 3-5 mm into the muscle before recording. The EMG signal was unreservedly activated and a foreordained age of five seconds was gained, bandpass separated at 3 Hz to 10 KHz, and tested at 20 KHz with 12 piece goals. The sign was then low pass sifted at 8 KHz. (Ho-Lim Choi et al., 2000) utilized four movements like stand up, plunk down, right advance, and left step. For each movement, he estimated EMG flags more than multiple times, and each movement was examined at a 2-kHz testing recurrence with a bandpass channel from 20 Hz to 350 Hz for 3s Hz. (Kevin Englehart et al., 2001) proposed band pass pre-preparing procedures for improving precision of the framework. Six distinct movement groups were generated in each topic: hand closure, opening of hands, wrist flexing, bracelet extension, spiralling bracelet deviation and ulno wrist deviation. Input from the 11 normally limbo people was collected, reported from the average hand, top, horizontal and base of the lower arm of four channels of Myoelectric Signal (MES). The Ag-AgCl terminals divided into 2 cm were procured for each bipolar tube. Checked at 1,000 Hz, each record was 256 ms in length, prefiltered somewhere in the range of 10 and 500 Hz.

(M Zecca et al., 2002) utilized band pass channel with cut-off recurrence fluctuated from 250 to 2000 Hz for constrict development antiquities and the insecurity of the cathode skin interface. A step filter at 50 or 60 Hz was utilized for expel power line commotion. Ten different hand developments were separated by applying anode over the lower arm muscles. Just two-channel framework was utilized for breaking down EMG signal from three typical subjects. 8 channels were conveyed for 12 hand and wrist developments for recording by (Reza Boostani et al., 2003). The signs were taken from ten handicapped individuals. Testing rate was 2975 Hz and signs were Butterworth's 9-request low pass philtre has been used to maximise their efficiency. Classified arm growth (Xiao Hu et al., 2004) as elbow flexion, elbow extension, lower arm pronation, and inner revolution of the shoulder. The biceps, triceps, and brachioradials and deltoid muscles were mounted on six channel bipolar anodes. The test was

witnessed by three daily volunteers. The repeat of research was measured as 256 Hz and the data was filtered with the tape transfer (3-120 Hz). (Mina Agarabi et al., 2004) recorded EMG signals from 21 sound subjects. EMG sensors were mounted at lower arm muscles. Various methods for holding the PC mouse like rest, side grasp and get position were tried. The sEMG signal was then sifted at a transfer speed of 20 to 450 Hz and tested at 1024 Hz.

(Jun-Uk Chu et al., 2005) broke down Self-Organizing Feature Map and Component Analysis (PCA) for dimensionality reduction and non-linear mapping of EMG signal. Nine kind of hand movement, flexion and brace expansion, spiral and ulnar bracelet flexion, pronation and wrist supination, The fingers were opened and handled and the analysis took unwinding. EMG signalling from digitator, carpal radial extensor, palmaris longus and carpal ulnar flashcraft has been estimated. The repeat test was set to 1024 Hz. Clamor was filtered out by 10 to 450 Hz bandwidth canal and a 100 dB gain enhancer. At that point, they were rectified and filtered out during that time request Butterworth filter cut-off recurrence 1 Hz, and re-examined with a 100 Hz inspecting recurrence. Seven anodes (L=6: six in the correct lower arm and one in the left lower arm) were utilized to lead pointer control tests. The data on click occasions was removed from the EMG signal estimated at the left lower arm. The length of the preparation information was  $T = 20$  and 2 examples of the learning information were utilized for each base bearing.

(Shalu George K et al., 2007) got EMG signals from five solid subjects in the age gathering of 21 to 25 years, utilizing Ag-AgCl surface anodes pre-gelled from the right hand biceps brachii. Sujets were approached in order to actively limit the affected muscle with two distinct paces. The testing recurrence was 2000 Hz. Band pass channel between 10-450 Hz was utilized for pre-preparing EMG signals. (Keisuke Shima et al., 2007) estimated EMG flags on five solid male subjects and one male furthest point amputee. An amputee lost approximately 3 cm from his left wrist of his lower arm. In four regions, it measured the EMG for carpal ulnar, brachioradialis, carpal radialis, and carpal radialis by Four Ag / AgCl Terminals sets (GE Marquette Corp., SEB120 framework,) in all regions. The EMG was registered on a 1 kHz test recurrence and a consistently low way philtre has been filtered. . The subject was approached to play out the accompanying four movements consistently for five-second time spans in the provided request: hand opening, hand getting a handle on, wrist expansion, and wrist flexion. EMG signals estimated from 25 patients with Parkinson's ailment and 22 sound subjects for controlling mechanical arm were proposed by (Saara Rissanen et al., 2007). Inspecting rate was fixed as 1000 and Butterworth band pass filler in the scope of 1-500 Hz. During the estimations, subjects were approached to hold their elbows at an edge of 90 degrees with their palms up. Karhunen-Loeve Transform (KLT) was utilized for dimensionality decrease. (Ryan J. Smith et al., 2008) proposed persistent deciphering of finger position for controlling fueled prostheses. 64 channel enhancer was applied for signal account with an inspecting pace of 2000 Hz. The subject was approached to move a solitary finger while keeping up the rest of the bit of the submit an impartial position. Signs were band constrained between 10 Hz and 500 Hz using an inline channel. (G. Fele-Zorz et al., 2008) proposed an examination among direct and non-straight sign preparing methods. Band-pass Butterworth filters were tried: 0.08-4, 0.3-4, and 0.3-3 Hz. Information were gathered from the stomach surface utilizing four AgCl2 terminals.

(Gurmanik Kaur et al., 2009) proposed Discrete Wavelets Transform (DWT) division strategies for EMG Signals. A total of 12 EMG signals were received from three usual subjects, five myopathic subjects and four subjects affected by engine neurons. . These EMG signals are basic 3-10 KHz band passes, inspected at 20 KHz for 12-piece objectives and consequently low 8 KHz separate passes. 6-th request Butterworth band-pass channel and cut-off recurrence of 20-500 Hz was utilized to evacuate the clamor. (Yannick Bastiaensen et al., 2009) applied band pass filtering between 10 to 500 Hz for upgrading sEMG signal. He likewise depicted how to utilize wavelet changes to dissect this sign in time and recurrence range, which gave us much more data than Fast Fourier Transform (FFT). EMG signal examined pace of at any rate 500 Hz. (Gurmanik Kaur et al., 2009) utilized band pass channel for commotion concealment.. Signs have been acquired for 5 seconds using 3 common subjects of the regular concentric needle cathode, Five myopathic subjects and four ill subjects of the engine neuron. EMG was a basic 3-10 KHz band pass, measured at 20 KHz with 12-piece targets and then with a low 8 KHz cross pass. (Nan Bu et al., 2009) utilized Bayesian Network (BN) for crossover movement classification approach. Four male subjects willfully partook in these tests. In positions of flexor carpi radialis, carpi ulnaris extender, bending carpi ulnar, and biceps brachii muscles, five cathods were connected to the client's lower and upper arm. On the flexor carpi radialis two sets of anodes have been added and one set per one. A telemetry framework (MT11, NEC Medical Systems Corporation) has enhanced the differential EMG signals. The Butterworth philtre's cutoff recurrence was 1 Hz and the EMG At the 1 kHz inspection recurrence, signals were reported. This test was performed by hand opening, handle, flexion, augmentation, pronation, and supination. (Claudio Castellini et al., 2009) utilized four hand developments like thumb, record, center and ring for sEMG hand prosthesis utilizing National Instruments DAQPCI-6023E applied for signal obtaining and testing rate was fixed at 256 Hz. The ten EMG cathodes were

applied to the subject's correct lower arm and held set up by versatile groups. A five conceivable classification was built up: no activity, handle by restricting the thumb and list finger, contradicting thumb and center, restricting thumb and ring, handle by contradicting the thumb and all other finger. A score and band pass channel was applied for signal enchaining.

Six high appendage gestures such as wrist flexion, extension of the hand, closed hand, open hand, pronation of the low arm and the lower arm supination have been investigated (Angkoon Phinyomark et al., 2009). SEMG signals were reported by two groups of Ag-AgCl red dab surface anodes on the right lower arm from flexor carpi radialis and extensor carpi radialis lengthus of a solid male. A 10-500 Hz transmitting band pass channel and an enhancer of 60 dB were used. Recurrence monitoring was set to 1 kHz using To-Advanced Single 16-piece Converter Board (DAQCard-6024E for national instruments). (Todd A. Kuiken et al., 2009) suggested the continuous myoelectrical regulation of fake arms in targeted muscle reinnervation (TMR). This vigilant TMR approach pushes the arm nerves to the choice of muscle destinations. These objective muscles develop EMG-flags, which can be weighed and used to control prosthetic braces, on the outside of the skin after reinnervation. 12 self-adhesive psychotic for each patient with TMR medication. Over the reinnerved muscles, EMG anodes were mounted on the skin. One anode has been mounted on the biceps, the other one on the triceps, and 6 on the lower proximal arm; 1 on the backside of the wrist; and 3 of them have been mounted on the right. In order for the EMG signals to be expelled from unwanted clamour, a band-pass between 5 to 400 Hz was increased. Knowledge at 1 kHz has been tested. The elbow flexion, elbow extension, wrist flexion, wrist were 11 inventions. Increase, wrist pronation, wrist supination, opening of the palm, three styles of handles and rest.

EMG information were procured from six subjects utilizing a 64-channel amplifier by (Francesco V. G. Tenore et al., 2009). Information were inspected at 2000 Hz and low-pass filtered at 500 Hz. Bipolar Ag-AgCl terminals were put regarding the matter's correct lower arm. Singular flexion and expansion developments of each finger (ten developments) were performed by each subject during signal securing. (Thiago V. Camata et al., 2010) broke down muscle exhaustion utilizing EMG. Eighteen prepared cyclists took an interest in this examination. 16-channel EMG with inspecting pace of 2000 Hz was utilized. The crude EMG signals were sifted utilizing a bandpass channel of 20 Hz and 500 Hz. (T. Lorrain et al., 2010) acquired signs utilizing wrist flexion, wrist augmentation, lower arm supination, lower arm pronation, thumb close performed by members. Six sets of Ag/AgCl surface terminals were mounted around the predominant lower arm at 1024 Hz inspecting rate. The sEMG information were separated somewhere in the range of 47 and 440 Hz.

(Hsiu-Jen Liu et al., 2010) recommended band pass channel and step channel for versatile upper-arm control framework. Two male and two female subjects were approached to flex and stretch out their upper arms to move the robot at 1 KHz testing rate. Two arrangements of terminals were put on the biceps brachii, triceps brachii separately. Electromagnetic clamor was around 60 Hz and was evacuated utilizing step channel and a 6th request band-pass Butterworth channel with the cut-off frequencies at 20 and 400 Hz was utilized for expelling other commotion. (Silvia Muceli et al., 2010) gathered information from four typically limbed people. Four exhibits were set around the circuit of the correct lower arm. The EMG signals were enhanced with an addition of 2000, tested at 2048 Hz. Preprocessing was completed by band-pass sifted with eighth request Bessel channel, data transfer capacity 10-750 Hz.

(Jakob R. Mathiesen et al., 2010) utilized sEMG and intramuscular EMG (iEMG) for expectation of getting a handle on power. The test included 11 sound subjects (4 female, 7 male) in the age of 22 to 26 years. The iEMG terminals were put in a bipolar configuration, in the muscle flexor digitorum profundus. All the while, sEMG was recorded in a bipolar configuration from a similar muscle. An amplification and filtering gadget (EM001-01 SMI) was utilized for both iEMG and sEMG. A wristband was utilized as a typical reference cathode. Testing recurrence was fixed as 20 kHz. The iEMG and sEMG were band pass filtered with frequencies 100-2500 Hz and 20-500 Hz. Two distinct information securing frameworks were utilized by (J Rafiee et al., 2011) to gather sEMG and intramuscular EMG signals. For surface EMG flags, a 16-anode straight cluster with bury terminal dividing of 2 cm was utilized. Each channel was filtered somewhere in the range of 10 and 500 Hz. For iEMG, needle cathodes were applied at pronator and supinator teres, flexor digitorum sublimas, extensor digitorum communis, flexor and extensor carpi ulnaris muscles. Six subjects performed ten hand developments for 5 sec each, with a 2 min resting period after each activity. The subjects denied feeling exhausted during these activities. The considered hand movements incorporates lower arm pronation, lower arm supination, wrist flexion, wrist augmentation, wrist kidnapping, wrist adduction, key grasp, toss hold, spread fingers, and a rest state.

sEMG securing framework noraxon myosystem 1400L, 8-channel was utilized by (Amirreza Ziai et al., 2011) to procure signals from 11 sound participants. Signs were thusly high-pass separated utilizing a zero-slack Butterworth fourth order channel (30 Hz cut-off recurrence), so as to expel movement relic. Extensor carpi radialis longus, extensor digitorum communis, extensor carpi ulnaris, extensor carpi radialis brevis, flexor carpi radialis, palmaris longus, flexor digitorum superficialis, flexor carpi ulnaris muscles were conveyed for signal extraction. (Wilmer J. Lobato Malaver et al., 2011) utilized expansion, flexion and unwinding developments for controlling myoelectric prosthesis. Butterworth third order channel with cutoff recurrence of 20 Hz to 500 Hz was applied for signal charm. Step channel was utilized to dispose of 60 Hz segment. (Kuldeep Singh et al., 2011) got EMG signals from six sound male subjects old enough gathering between 35-40 years. Test rate was kept 8000 Hz and band pass separated at 70-250 Hz.

### III.DISCUSSION

sEMG signal end up being a helpful apparatus for different applications concerning clinical reason for analytic, sport science for execution improvement and injury location just as human-PC. It is seen from study from various papers testing rate fixed as 1000 HZ and band pass channel inside range 10 – 500 HZ is appropriate arrangement for recording EMG sign for better acknowledgment precision.

### IV.CONCLUSION

Study on sEMG is wide, going from plan of terminals, recording systems, examination strategies and application for different purposes. sEMG ought to be used particularly for clinical analysis since its non-obtrusive methodology makes it considerably more agreeable for subjects. Yet there is a ton to improve particularly on structure of recording gear. From the review, we inferred that testing rate 1000 HZ with band pass channel ranges from 10-5000 HZ is most appropriate for getting greatest precision from surface EMG.

### REFERENCES

- 1.Constantinos S. Pattichis, Christos N. Schizas, Lefkos T. Middleton, 1995. Neural Network Models in EMG Diagnosis. IEEE Transactions on Biomedical Engineering, 42(5): 486-496.
2. Kevin Englehart, Bernard Hudgins, Philip A. Parker, 2001. Wavelet Based Continuous Classification Scheme for Multifunction Myoelectric Control. IEEE Transaction Biomedical Engineering, 48(3): 302-311.
3. M. Zecca, S. Micera, M. C. Carrozza, P. Dario, 2002. Control of Multifunctional Prosthetic Hands by Processing the Electromyographic Signal. Biomedical Engineering, 30(4-6): 459-485.
4. Reza Boostani and Mohammad Hassan Moradi, 2003. Evaluation of the Forearm EMG Signal Features for the Control of a Prosthetic Hand. Physiological Measurement, 24(2): 309-319.
5. Xiao Hu and Valeriy Nenov, 2004. Multivariate AR Modeling of Electromyography for the Classification of Upper Arm Movements. Clinical Neurophysiology, 115(6): 1276-1287.
6. Jun-Uk Chu, Inhyuk Moon, Museong Mun, 2005. A Real-Time Pattern Recognition for Multifunction Myoelectric Hand Control. IEEE/RSJ International Conference on Intelligent Robots and Systems, 3511-3516.
7. Shalu George, K. K. S. Sivanandan, K. P. Mohandas, 2012. Fuzzy Logic and Probabilistic Neural Network for EMG Classification-A Comparative Study. International Journal of Engineering Research & Technology, 1(5): 1-7.
5. Emayavaramban, G., Amudha, A., Ramkumar, M. S., Divyapriya, S., & Nagaveni, P. (2020, November). Surface Electromyography Feature Extraction Techniques—A Review. In 2020 4th International Conference on Electronics, Communication and Aerospace Technology (ICECA) (pp. 441-446). IEEE.
6. Amudha, A., Ramkumar, M. S., Emayavaramban, G., Divyapriya, S., Nagaveni, P., Mansoor, V. M., & Sivaramkrishnan, M. (2020). Resonant converter L3C for E-vehicle for charging a PV battery. Materials Today: Proceedings.
7. Divyapriya, S., Vijayakumar, R., Ramkumar, M. S., Amudha, A., Nagaveni, P., Emayavaramban, G., & Mansoor, V. (2020, October). IoT Enabled Drip Irrigation System with Weather Forecasting. In 2020 Fourth International Conference on I-SMAC (IoT in Social, Mobile, Analytics and Cloud)(I-SMAC) (pp. 86-89). IEEE.
8. Amudha, A., Ramkumar, M. S., Vijayalakshmi, V. J., Emayavaramban, G., Mansoor, V., Divyapriya, S., & Nagaveni, P. (2020, October). Modeling, Simulation and Design of Luo Converter for DC Micro Grid Application. In 2020 Fourth International Conference on I-SMAC (IoT in Social, Mobile, Analytics and Cloud)(I-SMAC) (pp. 1250-1256). IEEE.
9. Ramkumar, M. S., Amudha, A., Sivaramkrishnan, M., Divyapriya, S., Nagaveni, P., Emayavaramban, G., & Mansoor, V. (2020, October). Micro Grid based Low Price Residential Home to Grid-Modeling and Control of Power Management System. In 2020 Fourth International Conference on I-SMAC (IoT in Social, Mobile, Analytics and Cloud)(I-SMAC) (pp. 1179-1183). IEEE.
10. Rajakumari, R. F., & Ramkumar, M. S. (2020). Design considerations and performance analysis based on ripple

factors and switching loss for converter techniques. *Materials Today: Proceedings*.

11. Divyapriya, S., Emayavaramban, G., Amudha, A., Ramkumar, M. S., Nagaveni, P., & Mansoor, V. M. (2020). Internet of things enabled plug in electrical vehicle based self maximum demand controller for shopping mall. *Materials Today: Proceedings*.
12. Emayavaramban, G., Divyapriya, S., Mansoor, V. M., Amudha, A., Ramkumar, M. S., Nagaveni, P., & SivaramKrishnan, M. (2020). SEMG based classification of hand gestures using artificial neural network. *Materials Today: Proceedings*.
13. Ramkumar, M. S., Amudha, A., Nagaveni, P., Emayavaramban, G., Divyapriya, S., Mansoor, V. M., ... & Kavitha, D. (2020). Analysed results of DC-DC converters with softswitching techniques. *Materials Today: Proceedings*.
14. Mansoor, V. M., Nagaveni, P., Amudha, A., Divyapriya, S., Emayavaramban, G., Ramkumar, M. S., & SivaramKrishnan, M. (2020). Throwing light on lightning. *Materials Today: Proceedings*.
15. Krishnan, M. S., Dhevi, S. K., & Ramkumar, M. S. (2014). Power Quality Analysis in Hybrid Energy Generation System. *International Journal*, 2(1).
16. Krishnan, M. S., Amudha, A., & Ramkumar, M. S. (2018). Execution Examination Of Three Phase Ac To Three Phase Ac Matrix Converter Using Distinctive Transporter Based Exchanging Algorithms. *International journal of Pure and Applied Mathematics*, 118(11), 609-617.
17. Krishnan, M. S., Sriragavi, S., & Ramkumar, M. S. (2017). Impedance Source Inverter and Permanent Magnet Synchronous Generator For Variable Speed Wind Turbine. *International Journal of Computer & Mathematical Sciences (IJCMS)*, 6(9), 98-105.
18. Sivakumar, N., Kavitha, D., Ramkumar, M. S., Bhavithira, V., & Kalaiarasi, S. (2017). A Single Stage High Gain Converter For Grid Interconnected Renewable Application Using Perturb And Observe. *International Journal of Control Theory and Applications (IJCTA)* 10 (38) 161, 175.
19. Govindaraju, K., Bhavithira, V., Kavitha, D., Kuppusamy, S., & Balachander, K. Improvement of Voltage Profile and Loss Minimization in IEEE 14 Bus System using FACTS Devices. *International Journal of Control Theory and Applications*, ISSN, 0974-5572.
20. Sownthara, M., & Ramkumar, M. S. (2014). Wireless Communication Module To Replace Resolver Cable In Welding Robot. *International Journal of Advanced Information Science and Technology* on, 23(23), 230-235.
21. Krishnan, M. S., Ramkumar, M. S., & Sownthara, M. (2014). Power management of hybrid renewable energy system by frequency deviation control. *Int. J. Innov. Res. Sci. Eng. Technol*, 3(3), 763-769.
22. R.Sudhakar and M.Siva Ramkumar "Boosting With SEPIC" in 'International Journal of Engineering and Science' 3 (4) pp 14-19, 2014.
23. Emayavaramban, G., Divyapriya, S., Mansoor, V. M., Amudha, A., Ramkumar, M. S., Nagaveni, P., & SivaramKrishnan, M. (2020). SEMG based classification of hand gestures using artificial neural network. *Materials Today: Proceedings*.
24. Amudha, A., Ramkumar, M. S., & Krishnan, M. S. (2017). Perturb and Observe Based Photovoltaic Power Generation System For Off-Grid Using Sepic Converter. *International Journal of Pure and Applied Mathematics*, 114(7), 619-628.
25. Fang, S., Hussein, A. F., Ramkumar, S., Dhanalakshmi, K. S., & Emayavaramban, G. (2019). Prospects of electrooculography in human-computer interface based neural rehabilitation for neural repair patients. *IEEE Access*, 7, 25506-25515.
26. Emayavaramban, G., Divyapriya, S., Mansoor, V. M., Amudha, A., Ramkumar, M. S., Nagaveni, P., & SivaramKrishnan, M. (2020). SEMG based classification of hand gestures using artificial neural network. *Materials Today: Proceedings*.
27. Ramkumar, S., Emayavaramban, G., Kumar, K. S., Navamani, J. M. A., Maheswari, K., & Priya, P. P. A. (2020). Task Identification System for Elderly Paralyzed Patients Using Electrooculography and Neural Networks. In *EAI International Conference on Big Data Innovation for Sustainable Cognitive Computing* (pp. 151-161). Springer, Cham.
28. Anitha, T., Shanthi, N., Sathiyasheelan, R., Emayavaramban, G., & Rajendran, T. (2019). Brain-computer interface for persons with motor disabilities-A review. *The Open Biomedical Engineering Journal*, 13(1).
29. Kumar, S. S., Kavitha, D., Amudha, A., Emayavaramban, G., & Ramkumar, M. S. (2019). Analysis Of New Novelty Multilevel Inverter Configuration With Boost Converters For A Photovoltaic System With MPPT. *Mathematical & Computational Forestry & Natural Resource Sciences*, 11(1).
30. Gurmanik Kaur, Ajat Shatru Arora, V.K. Jain, 2009. Comparison of the Techniques Used for Segmentation of EMG Signals. *11th WSEAS International Conference on Mathematical and Computational Methods*, 124-129.
31. Angkoon Phinyomark, Chusak Limsakul, Pornchai Phukpattaranont, 2009. A Novel Feature Extraction for Robust EMG Pattern Recognition. *Journal of Computing*, 1(1): 71-80.
32. Jakob R. Mathiesen, Mette F. Bog, Ema Erkocevic, Marko J. Niemeier, Anne Smidstrup, Ernest N. Kamavuako,

2010. Prediction of Grasping Force Based on Features of Surface and Intramuscular EMG. 7th Semester Conference Paper, 1-9.
33. Wilmer J. Lobato Malaver and Sergio Salas Arriaran, 2011. Virtual Simulation of a Myoelectric Prosthesis. INNS International Educational Symposium on Neural Networks, 1-9.33.
34. Kuldeep Singh, Richa Bhatia, Hardeep S. Ryait, 2011. Precise and Accurate Multifunctional Prosthesis Control Based on Fuzzy Logic Techniques. International Conference on Communication Systems and Network Technologies, 188-193.